

# Auto-segmentation of structures in cervical cancer treatment planning using a deep learning framework

S. Chacko<sup>1</sup>, C. Sjogreen Blanco, PhD<sup>1</sup>, J. Parameshwaran, MD<sup>1</sup>, L. Court, PhD<sup>1</sup>, T. Netherton, PhD, DMP<sup>1</sup>

<sup>1</sup>Department of Radiation Physics, The University of Texas MD Anderson Cancer Center, Houston, Texas, USA

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### Purpose

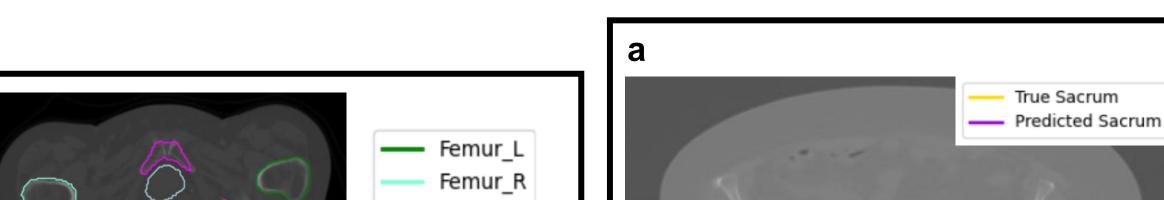
We seek to evaluate whether the lean deep learning PocketNet model yields results comparable to the larger nnU-Net model in the automated segmentation of clinical target volumes and pelvic organs in CT imaging of cervical cancer patients.

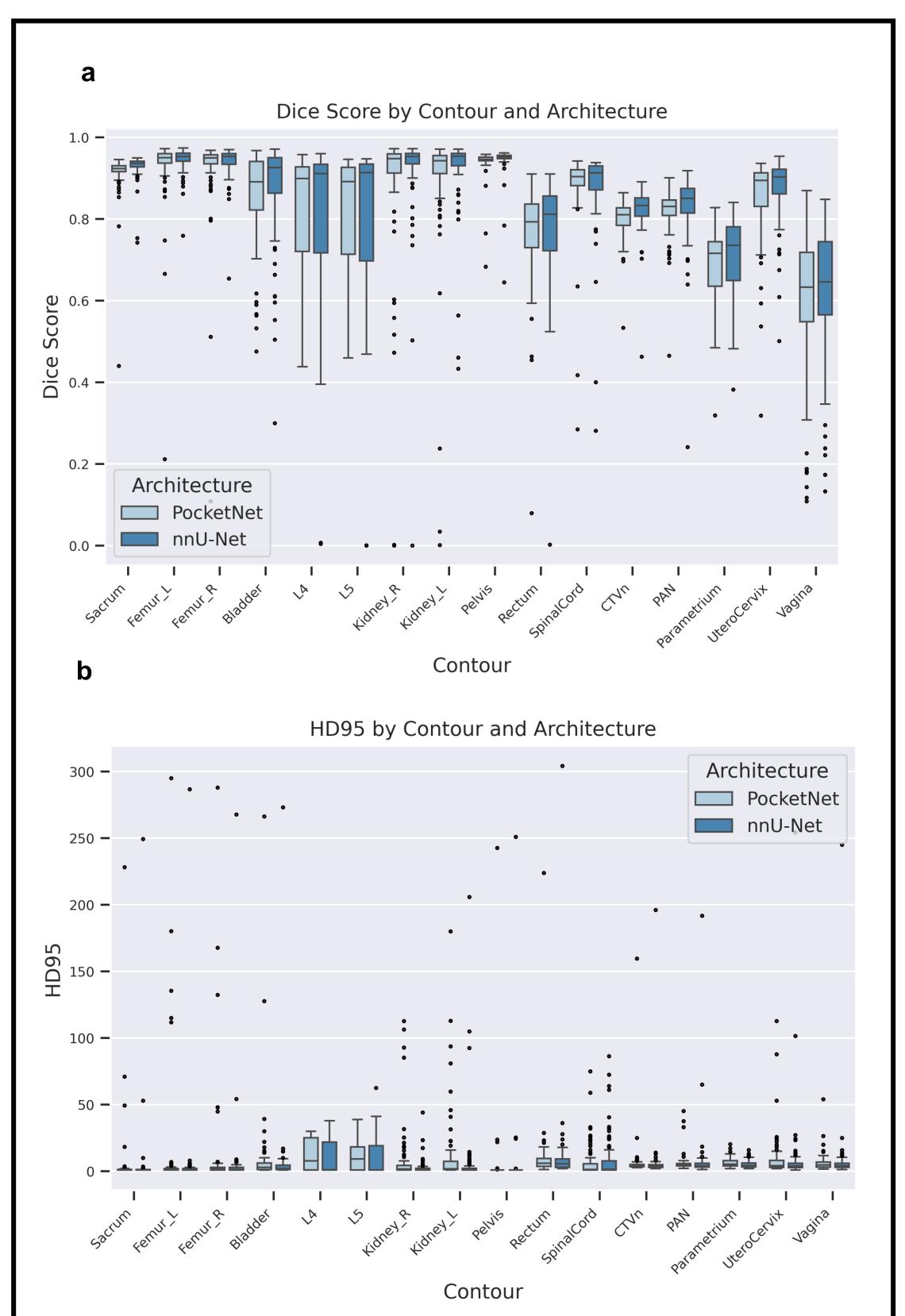
### Introduction

- Cervical cancer is the fourth most prevalent cancer in women worldwide, primarily due to infection with human papillomavirus (HPV).
- Radiotherapy workflow requires manual contouring of tumor volumes and pelvic organs, but this process is time-consuming and resource-intensive. Automatic segmentation of medical images has been proposed to address these shortcomings. Convolutional neural networks (CNNs) are the first-line choice of deep learning model architecture for this task. The U-Net form, with its symmetric contractile and expansive paths, is best suited for the pixel-by-pixel classification and image localization.<sup>1</sup> U-Net optimization led to the creation of PocketNet, a lightweight model with reduced parameters designed to operate in lowresource environments.<sup>2</sup> Another variant, nnU-Net, was designed with the intention of automatically configuring itself to address cumbersome manual tuning of parameters.<sup>3</sup>

## Results

- The nnU-Net model achieved mean Dice scores > 0.70 for all structures except the vagina, and a mean Dice score > .90 for the sacrum, femurs, and pelvis (Figure 3).
- The PocketNet model achieved mean Dice scores > 0.70 for all structures except the vagina and parametrium, and a mean Dice score > .90 for the sacrum, femurs, and pelvis (Figure 3).
- Results from the Wilcoxon signed-rank test revealed that nnU-Net performed better than PocketNet for auto-segmentation of the sacrum, bladder, L4, L5, kidneys, pelvis, CTVn, PAN, parametrium, and utero-cervix (Figure 4).





## **Methods**

### Autocontouring

- The dataset consisted of 82 abdominal CT scans of patients who received radiotherapy.
- Four structures were specifically delineated by a radiologist according to consensus guidelines, the remaining 12 were clinically approved structures used from treatment planning.
   A custom preprocessing pipeline was applied to remove overlap between structures using manually-defined set of rules. These masks were then compiled into a single file to train the model (Figure 1).
   Models with nnU-Net and PocketNet architectures were trained on 92 cases, accompanied by 5-fold cross validation.

	Femur_R Bladder Pelvis Rectum	b
		19
Contour	p-value	all in
Sacrum	3.15E-13	and the second se
Femur_L	3.44E-03	and the second second
Femur_R	3.44E-03	
Bladder	7.78E-07	100000000000000000000000000000000000000
L4	1.74E-01	
L5	6.55E-02	
Kidney_R	7.10E-06	C C
Kidney_L	3.97E-06	the state of the
Pelvis	1.28E-13	
Rectum	5.08E-03	
Spinal Cord	6.43E-03	
CTVn	1.66E-11	A CONTRACTOR
PAN	1.04E-04	A COLORADOR
Parametrium	7.97E-06	and the second second
Utero-Cervix	4.52E-07	
Vagina	8.66E-04	
		Figure 2 \

**Figure 4. Wilcoxon-signed rank test.** Differences in Dice values from the median are captured with p-values, which confirms a difference in model performance by contour.

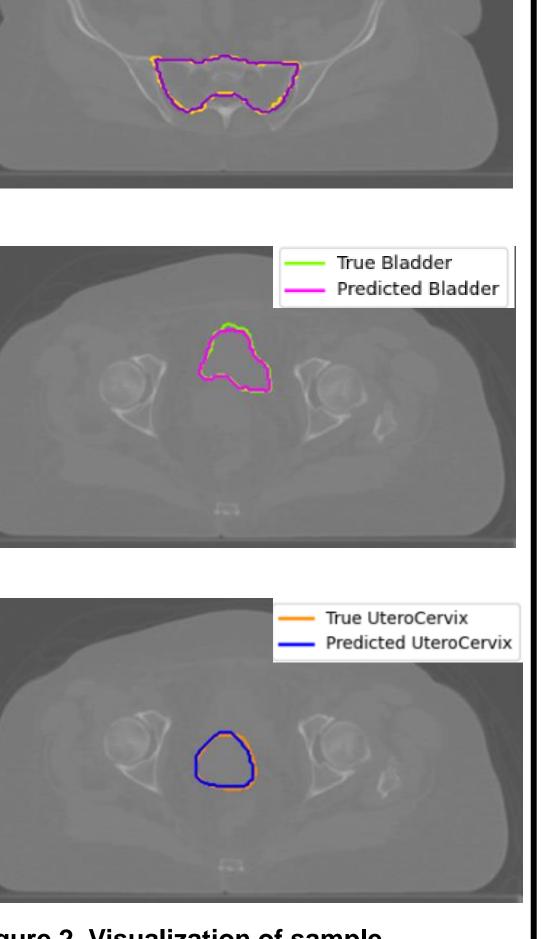


Figure 2. Visualization of sample predicted contours against their ground truth equivalent. Sample contours from the (a) bony, (b) soft tissue organs, (c) target subgroups are plotted.

Figure 3. Quantitative performance compared between both models. (a) Mean DSC and (b) HD95 were calculated for each predicted contour against its ground truth delineation.

### Quantitative evaluation

- The model performances were evaluated through calculation of the Dice-Sorensen coefficient (DSC) and 95<sup>th</sup> percentile Hausdorff distance (HD95) per predicted contour.
- The Dice metric was compared between models using a one-sided Wilcoxon signedrank test (p < 0.05).</li>

#### RCR

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# Discussion

- Both PocketNet and nnU-Net have a stronger performance on bony structures and a weaker performance on soft tissue organs and target structures.
  - There is lower contrast for anatomical boundaries on CT images between soft tissue organs, so it is harder to differentiate compared to MRI images.
  - Higher contrast in bony structures allows for easier differentiation on CT.
  - Both models achieved better accuracy at the center of structures, as opposed to the boundaries.
- nnU-Net performed significantly better than PocketNet at segmentation for most structures,
- More work must be done in model optimization to differentiate between soft tissue densities on CT imaging, namely in the vagina and parametrium structures.
- A more detailed qualitative analysis of the outliers will be conducted to evaluate model weaknesses.
- Future work will involve physician review of model results to corroborate these findings in a clinical context. Testing clinical acceptability of contours will
  determine whether the discrepancy in performance is patent in a clinical context, and whether PocketNet outputs can be sufficient in low-resource settings.

### Conclusions

- Both PocketNet and nnU-Net architectures can successfully and reliably auto-contour pelvic structures and tumor volumes.
- nnU-Net predicted certain structures significantly better (p < 0.05) than PocketNet at the cost of greater computational power.

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